

Heterogeneous Diffusion of a Membrane-Bound pHLIP Peptide

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ABSTRACT Lateral diffusion of cell membrane constituents is a prerequisite for many biological functions. However, the diffusivity (or mobility) of a membrane-bound species can be influenced by many factors. To provide a better understanding of how the conformation and location of a membrane-bound biological molecule affect its mobility, herein we study the diffusion properties of a pH low insertion peptide (pHLIP) in model membranes using fluorescence correlation spectroscopy. It is found that when the pHLIP peptide is located on the membrane surface, its lateral diffusion is characterized by a distribution of diffusion times, the characteristic of which depends on the peptide/lipid ratio. Whereas, under conditions where pHLIP adopts a well-defined transmembrane α -helical conformation the peptide still exhibits heterogeneous diffusion, the distribution of diffusion times is found to be independent of the peptide/lipid ratio. Taken together, these results indicate that the mobility of a membrane-bound species is sensitive to its conformation and location and that diffusion measurement could provide useful information regarding the conformational distribution of membrane-bound peptides. Furthermore, the observation that the mobility of a membrane-bound species depends on its concentration may have important implications for diffusion-controlled reactions taking place in membranes.

INTRODUCTION

The lateral diffusion of lipids and absorbed biomolecules (e.g., proteins and peptides) in cell membranes is thought to play an important role in many biological processes as it may control the timescale within which key molecular events take place (1–6). For example, to form the functional oligomeric structures, membrane-bound antimicrobial peptides have to diffuse laterally to find each other. Thus, in this case the diffusion rate of the membrane-bound peptides may limit the rate of oligomer formation. Similarly, the lateral diffusion rate of membrane-bound α -helices may play an important role in determining the folding time of membrane proteins, as the two-state model of membrane protein folding (7) suggests that secondary structure formation precedes the formation of tertiary structures. Because of its importance, many studies have been performed to examine the diffusion properties of membrane-bound biological molecules (8–41).

Although these studies have demonstrated that the charge, size, and molecular shape of the diffusing species are important determinants of its diffusivity, many factors still remain unexplored. For example, the diffusion of a membrane-bound species could be significantly influenced by its conformation, location, and concentration. Among these potential influences, the effect of concentration is particularly worthwhile to investigate, as such effects would have important implications for interpreting the kinetics of diffusion-controlled reactions. Herein, in an attempt to provide further insight into factors that affect the diffusion of membrane-bound peptides, we measure the diffusivity of a pH (low) inserting peptide (pHLIP) in model membranes under different conditions using fluorescence correlation spectroscopy (FCS).

The pHLIP peptide used in this study is based on that designed by Engelman and co-workers (42–47). Our motives for choosing this peptide include the following:

1. The interaction of pHLIP with model membranes is well studied and understood (46–48).
2. The conformation and location of membrane-bound pHLIP molecules can be easily controlled by changing the solution pH: near neutral pH, the pHLIP binds to membrane surface as an extended chain, whereas at low pH it forms a transmembrane (TM) α -helix due to protonation of the aspartic acid residues.
3. Perhaps most importantly, unlike antimicrobial peptides, the membrane-bound pHLIP molecules remain monomeric and do not induce membrane fusion or damage even at high peptide/lipid ratios.

Taken together, these unique membrane-binding properties of pHLIP make it an ideal model system to probe how those aforementioned factors affect the diffusion of membrane-bound peptides.

Fluorescence correlation spectroscopy (FCS) is based on correlating fluorescence intensity fluctuations arising from fluorescent molecules diffusing in and out of a small confocal volume, thus providing a convenient means to measure the diffusion time and hence the diffusion constant of the diffusing species (49,50). In addition, FCS allows observation of single molecules, and thus can be used to probe diffusion heterogeneity (51–53). Indeed, our results show that the diffusion of pHLIP in two model membranes, namely, supported lipid bilayers and giant unilamellar vesicles (GUVs), is heterogeneous and that the extent of the heterogeneity depends on pH and peptide concentration. Interestingly, the diffusion time distribution of the surface-bound pHLIP consists of two distinct peaks at high peptide/lipid ratios,

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indicating the feasibility of using FCS to probe the conformational distribution of membrane-bound peptides and proteins.

MATERIALS AND METHODS

Materials

All materials were used as received. Fmoc-protected amino acids were purchased from Advanced Chem Tech (Louisville, KY). Rink amide PEGA resin was purchased from Novabiochem (San Diego, CA). Tetramethylrhodamine-5-maleimide (TMR-maleimide) was purchased from AnaSpec (San Jose, CA). Phospholipid 1-palmitoyl-2-oleoyl phosphatidylcholine (POPC) and 1-palmitoyl-2-oleoyl-phosphatidylglycerol (POPG) was purchased from Avanti Polar Lipids (Alabaster, AL). 2-[methoxy(polyethyleneoxy)propyl] trimethoxysilane (PEG) was purchased from Gelest (Morrisville, PA). Texas Red 1,2-dihexadecanoyl-*sn*-glycero-3-phosphoethanolamine, triethylammonium salt (Texas-Red-DHPE) was purchased from Molecular Probes (Eugene, OR).

Peptide synthesis and labeling

The pHLIP peptide (sequence: ACEQNPIYWARYADWLFTPLLLL DLALLVDADEGTG) was synthesized using standard Fmoc-based solid-phase synthesis protocols employing a double-coupling strategy on a PS3 peptide synthesizer (Protein Technologies, Boston, MA) and purified by reverse-phase HPLC (1100 Series; Agilent Technologies, Quantum Analytics, Foster City, CA). The identity of the peptide was verified by MALDI-TOF mass spectrometry. The fluorescence probe, TMR-maleimide (AnaSpec), was attached to the peptide via the cysteine residue and the resultant TMR-labeled peptide product was further purified using a G-10 size-exclusion column.

Preparation of supported lipid bilayers and giant unilamellar vesicles

All membranes were made from POPC. Specifically, supported lipid bilayers were prepared from a pre-prepared POPC vesicle solution (2 mg/mL lipid and 10 mM phosphate buffer, pH 8.0 or 4.0). First, an aliquot (80 μ L) of this vesicle solution was pipetted into a preheated (40°C) petri dish, and then a dry, PEG-covered glass-slip was placed on top of the vesicle solution. This assembly was further incubated at 40°C for ~30 min, allowing for the formation of the lipid bilayer on top of the PEG surface of the glass-slip. Then the glass-slip was carefully removed from the bottom of the petri dish and rinsed out by copious phosphate buffer to remove any nonfused vesicles.

Giant unilamellar vesicles (GUVs) were prepared by the standard method of electrosweating (54) using a custom-made closed perfusion chamber and indium-tin-oxide (ITO) coated coverslips (Delta Technologies, Stillwater, MN) as electrodes. Briefly, 100 μ L of 1 μ M/mL POPC or POPC/POPG (3/1, mol/mol) lipid mixture solution in chloroform was first deposited on an ITO coverslip. After evaporation of the solvent, the chamber was assembled from two lipid-coated ITO coverslips separated by a rubber spacer and filled with 100 mM sucrose solution. A voltage of 1.2 V/mm at a frequency of 5 Hz was applied to the system for 2 h while incubating the chamber at 60°C. The final pH of the GUV solution (50 mM phosphate buffer) was adjusted to either 4.0 or 8.0. Same procedures were used to prepare POPC GUVs containing Texas Red-DHPE. The only difference is that the 1 μ M/mL POPC chloroform solution also contains 0.002 mol % Texas Red-DHPE.

FCS sample preparation

For experiments conducted with supported lipid bilayers, a 30 μ L peptide stock solution at the desired concentration and pH (4 or 8, 50 mM phosphate buffer) was added on top of the supported lipid bilayer and allowed to equilibrate for 1 h before FCS measurements. In all cases, the concentration of the TMR-labeled pHLIP in the peptide stock solution is 1 nM.

For experiments involving GUVs, the sample solution was prepared by mixing equal volumes of a peptide solution at the desired concentration and pH (50 mM phosphate buffer) and a GUV suspension in 100 mM sucrose solution. This mixed solution was then introduced into a custom-made, sealed FCS sample chamber and was allowed to equilibrate for 2 h, during which the GUVs settled to the bottom of the coverslip and remained stationary over the course of the experiment. For measurements involving 0.1 and 1 nM peptide, only TMR-labeled pHLIP was used. In all other cases, both labeled and unlabeled peptides were used, and the concentration of the labeled peptide was maintained at 1 nM. Finally, for diffusion measurements of the lipids (i.e., Texas Red-DHPE), only unlabeled peptides were used.

FCS setup and data analysis

The detail of the FCS apparatus has been described elsewhere (55). In this study, each FCS curve (1 μ s–10 s) measuring the diffusion of the membrane-bound TMR-labeled pHLIP peptides was obtained by correlating the fluorescence signals for a duration of 40 s and further fit to the equation

$$G(\tau) = \frac{1}{N} \left(\left(\frac{f_a}{1 + \frac{\tau}{\tau_D^a}} \right) + \left(\frac{f_b}{1 + \frac{\tau}{\tau_D^b}} \right) \left(\frac{1}{1 + \frac{\tau}{\omega^2 \tau_D^b}} \right)^{1/2} \right) \times \left(\frac{1 - T + T \times e^{-\frac{\tau}{\tau_{\text{triplet}}}}}{1 - T} \right), \quad (1)$$

where τ_D^a represents the characteristic two-dimensional diffusion time constant of membrane-bound species, and τ_D^b represents the three-dimensional diffusion time constant of unbound species in solution, which was determined from the diffusion of TMR-labeled pHLIP in buffer solution (see below). In all cases, we found that f_b was <10%. Thus, only the two-dimensional diffusion time constants were considered and discussed in the Result and Discussion sections. Specifically, they were presented in the format of probability distribution, wherein the data were binned every 200 μ s, and also the format of cumulative distribution.

On the other hand, those FCS curves obtained with Texas Red-DHPE in membranes were fit to the following two-dimensional diffusion model:

$$G(\tau) = \left(\sum_{i=1}^n \frac{1}{N} \left(\frac{f_i}{1 + \frac{\tau}{\tau_D^i}} \right) \right) \times \left(\frac{1 - T + T \times e^{-\frac{\tau}{\tau_{\text{triplet}}}}}{1 - T} \right). \quad (2)$$

We found that for Texas Red-DHPE diffusion in membrane in the absence of pHLIP, all FCS curves can be adequately fit by a single diffusion component (i.e., $n = 1$). For Texas Red-DHPE diffusion in membrane in the presence of pHLIP, a small number of FCS curves required a second component (i.e., $n = 2$) to yield a good fit.

For those FCS curves obtained with TMR-labeled pHLIP in buffer solution, the following three-dimensional diffusion model was used to fit the data:

$$G(\tau) = \frac{1}{N} \left(\left(\frac{1}{1 + \frac{\tau}{\tau_D}} \right) \left(\frac{1}{1 + \frac{\tau}{\omega^2 \tau_D}} \right)^{1/2} \right) \times \left(\frac{1 - T + T \times e^{-\frac{\tau}{\tau_{\text{triplet}}}}}{1 - T} \right), \quad (3)$$

In all the equations above, ω refers to the axial/lateral dimension ratio of the confocal volume element, N represents the number of fluorescent

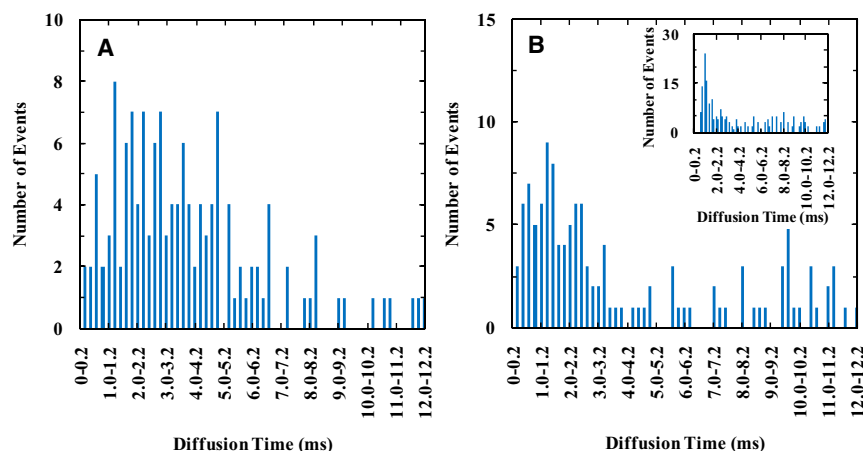


FIGURE 1 Diffusion time (τ_D) distributions of TMR-labeled pHLIP bound to a supported lipid bilayer of POPC at pH 8 and different total peptide concentrations: (A) 1 nM and (B) 1 μ M. (Inset) Diffusion time (τ_D) distribution of Texas Red-DHPE (0.002 mol %) in supported lipid bilayer of POPC at pH 8.

molecules in the confocal volume, f_i represents the fraction of the diffusion component i , τ_{triplet} is the triplet lifetime of the fluorophore, and T represents the corresponding triplet amplitude. The value of ω was determined using the diffusion coefficient and the measured diffusion time of the fluorescent dye, R6G, in water. A nonlinear least-squares curve-fitting algorithm, which uses Gauss-Newton approach for the initial search of the fitting parameters and then the method of gradient descent for a finer search, was used to fit all the FCS data without weighting. For each case, representative FCS curves and the corresponding fits and residuals were given in Fig. S1, Fig. S2, Fig. S3, Fig. S4, Fig. S5, Fig. S6, Fig. S7, Fig. S8, and Fig. S9, which can be found in the Supporting Material.

RESULT

Diffusion behavior of pHLIP bound to a supported lipid bilayer

Supported lipid bilayers provide a convenient two-dimensional membrane environment for diffusion measurements. Thus, we first investigated the diffusion properties of pHLIP molecules that are bound to a supported lipid bilayer as a function of peptide concentration. To reduce any potential interactions between the peptide and the microscope coverslip on which the lipid bilayer was prepared, a layer of PEG polymer was added between the glass surface and the bilayer. As shown (Fig. 1 A and Fig. S10 A), at pH 8 and relatively low peptide concentration, wherein the peptide remains unfolded and is located at the membrane surface (42–47), repeating FCS measurements, each with an acquisition time of 40 s, indicate that the diffusion of pHLIP is very heterogeneous. Interestingly, as indicated (Fig. 1 B and Fig. S10 B), increasing the peptide concentration appears to decrease the heterogeneity of the diffusion time (τ_D) and also leads to a decrease in the average diffusion time of the peptide. However, FCS measurements using a fluorescent-tracer-labeled lipid (i.e., Texas-Red-DHPE) in the absence of pHLIP showed that the diffusion of the lipid is heterogeneous (inset of Fig. 2 B). Although this result is in agreement with that of Burns et al. (51), it also suggests that the heterogeneous diffusion of pHLIP observed in the current case could arise from interactions between peptide and the substrate or between lipid and the substrate. Nevertheless, control experiments

showed that the characteristic diffusion times of pHLIP in buffer, obtained from multiple repeated measurements, are only distributed within a very narrow time range (Fig. 2). In addition, the diffusion constant of pHLIP in aqueous solution is determined to be $(1.3 \pm 0.1) \times 10^{-6} \text{ cm}^2/\text{s}$, which is consistent with those obtained on other peptides of similar size (56,57), whereas the modest decrease in the diffusion time at pH 4 compared to that at pH 8 is likely due to the increased hydrophobicity of the peptide upon protonation of the Asp residues. Thus, these control experiments suggest that a better model membrane is required to determine whether pHLIP exhibits heterogeneous diffusion when bound to membranes.

Diffusion behavior of pHLIP bound to GUVs

To eliminate any potential effects of the coverslip on the diffusion of the membrane-bound peptide, we carried out similar FCS measurements using GUVs consisting of either POPC or POPC/POPG mixture (3:1).

As shown (Fig. 3), the GUVs used in this study have a diameter of 5–50 μm and remain static on the timescale of the FCS experiments. Thus, by placing the focus of the

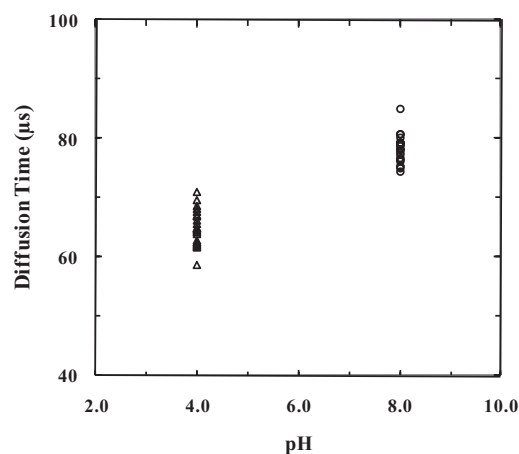


FIGURE 2 Diffusion times of TMR-labeled pHLIP in water at pH 4 and 8, respectively.

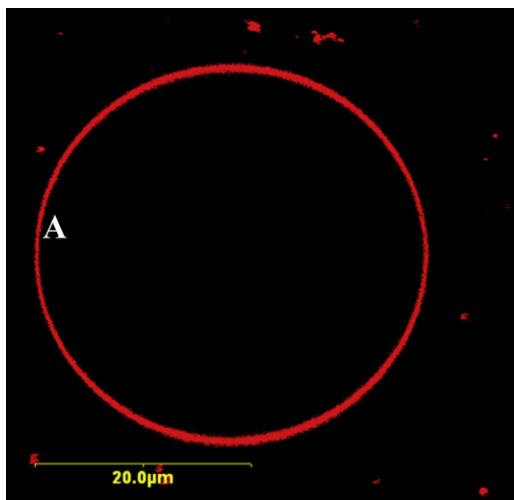


FIGURE 3 Confocal image of a representative POPC GUV. The fluorescence was derived from a small number of dye-labeled lipids (0.1 mol %, Texas Red-DHPE).

excitation laser beam near the center of the upper membrane of the GUV, any interference arising from the coverslip can be eliminated (58). Because membrane undulations/drift movements are known to introduce additional (or nondiffusion) components in the FCS curves (59), care has been taken to exclude those FCS curves that contain such interferences. This was achieved by rejecting those fluorescence traces that showed an apparent decrease in the counting rate (during the FCS measurement) that was reversible upon refocusing (58,60) and those FCS curves that exhibit a very long (i.e., >1 s) component (61). As shown (Fig. 4, A–C), for POPC membranes the diffusion times of pHLIP at pH 8 clearly show a distribution (hereafter referred to as τ_D -distribution) whose position and width depend on the peptide concentration or the peptide/lipid ratio. It is apparent that at relatively high concentration, the distribution becomes bimodal, and the average diffusion time becomes shorter. As indicated (Fig. S11 and Fig. S12), a similar concentration dependence is also observed for POPC/POPG membranes at pH 8 although the overall change is less pronounced. In stark contrast, at pH 4 the τ_D -distribution of pHLIP shows little or no dependence on peptide concentration (Fig. 4, D–F). Taken together, these results indicate that the location and conformation of a membrane-bound peptide are important determinants of its diffusibility.

To better understand these data and to serve as a control, we also measured the lipid diffusion times in the POPC GUV membrane using a fluorescent-tracer-labeled lipid (i.e., Texas-Red-DHPE) in the presence and absence of pHLIP. As shown (Fig. 5 and Fig. S13), the measured lipid diffusion times in the absence of the peptide are narrowly distributed at ~1.0 ms, indicating that the intrinsic lipid diffusion is more or less homogeneous. However, addition of the peptide affects the lipid diffusion in such a way that the mobility of the lipids depends on the concentration and location of

the peptide (Figs. 6 and 7, and Fig. S14 and Fig. S15). For example, at pH 8 and relatively high peptide concentration (Fig. 6 and Fig. S14), the τ_D -distribution clearly shows a longer component, as compared to that obtained in the absence of pHLIP.

DISCUSSION

While the diffusion of chemical constituents of cell membranes is of fundamental importance for many biological events and functions, very little is known about the timescale during which such diffusions occur and what affects their rate. Herein, we use a model peptide system (pHLIP) and FCS technique to investigate how the location, conformation, and concentration of the peptide affect its mobility in supported lipid bilayers and the membrane of GUVs. We find that even for such a relatively simple system, its diffusion is heterogeneous and shows complex dependence on those aforementioned factors.

Diffusion of pHLIP bound to membrane surface

At pH 8 and relatively low peptide concentrations (e.g., 0.1 nM), the lateral diffusion of pHLIP molecules on the membrane surface shows a broad τ_D -distribution (Fig. 4 A and Fig. S11 D), indicating the heterogeneous nature of the peptide's mobility. Previously it has been shown that FCS is able to follow protein unfolding transition (62) and that repeat FCS measurements are even capable of unmasking the conformational heterogeneity of unfolded proteins, provided that the unfolded conformers have distinctly different hydrodynamic radii and they interconvert slowly in comparison to their respective transit times (i.e., τ_D) through the confocal volume (63). The observation that the diffusion of pHLIP is characterized by a broad τ_D distribution indicates that the membrane-bound peptide samples an ensemble of slowly interconverting conformations. This picture is entirely consistent with the study of Engelman and co-workers (45), which showed that under similar conditions the surface-bound pHLIP adopts an ensemble of extended and unstructured conformations (45). In addition, a correlation existing between peptide conformation and diffusivity is readily explicable by the fact that the lateral mobility of a surface-bound molecule depends on the strength of its interactions with the membrane, a quantity directly related to the molecular conformation.

Of particular interest is that the (mean) diffusion time of the surface-bound pHLIP molecules depends on peptide concentration (or more precisely the peptide/lipid ratio), which could have important implications for non-unimolecular reactions. As shown (Fig. 4, A–C, and Fig. S11), increasing the peptide/lipid ratio results in a narrower τ_D -distribution and also a shift of the peak position of the distribution toward a shorter time for both POPC and POPC/POPG membranes. In addition, the τ_D -distribution obtained at high

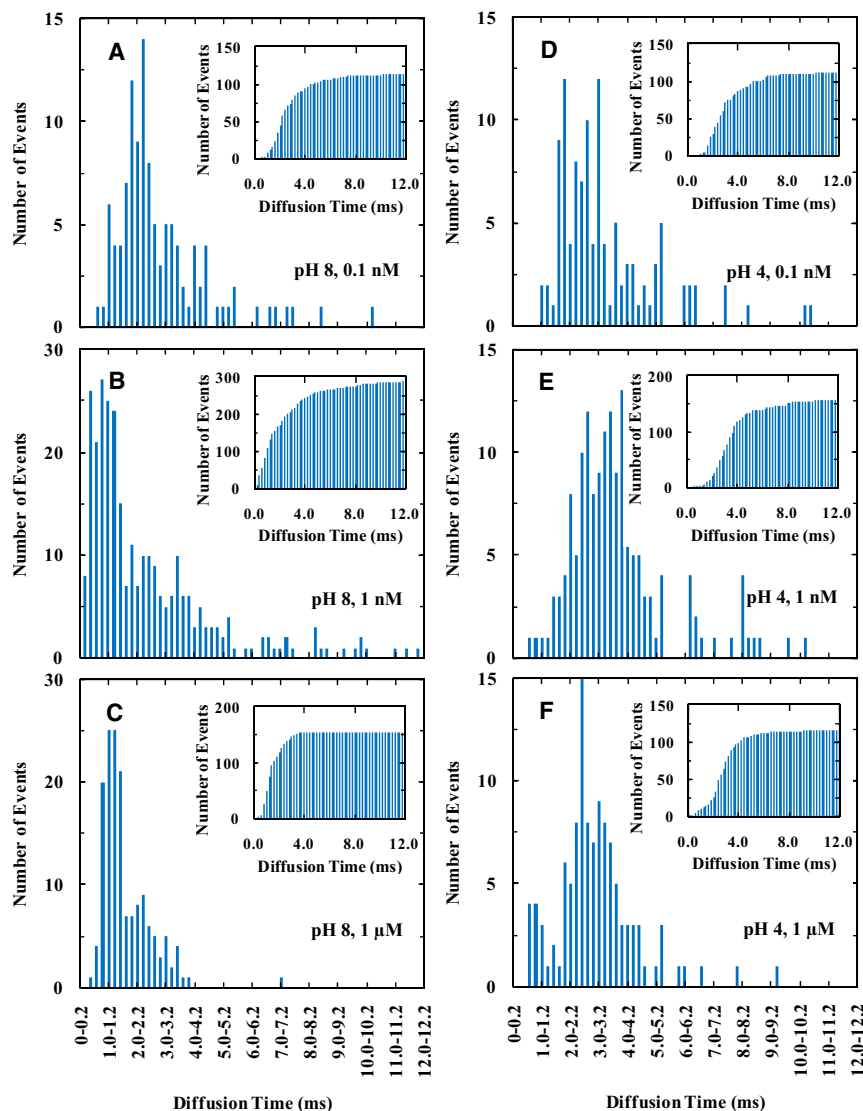


FIGURE 4 Diffusion time (τ_D) distributions of TMR-labeled pHLIP bound to the lipid bilayer of GUVs measured at different total peptide concentrations and pH values, as indicated. (Insets) Corresponding cumulative distribution of the diffusion times.

peptide concentrations can be described reasonably well by two components (Fig. 4 C), centered at ~ 1.0 and 2.5 ms for POPC membrane, respectively, indicating that the pHLIP molecules can sample (at least) two distinguishable conformational ensembles that interconvert slowly.

The diffusion behavior of surface-bound pHLIP at pH 8 can be understood in terms of peptide surface coverage. At low concentration (e.g., 0.1 nM), where the peptide surface coverage is low, peptide molecules rarely encounter each other. Thus, each can freely explore the entire conformational space determined by the underlying pHLIP-membrane interactions, generating a broad distribution of conformations (45), which in turn gives rise to a broad τ_D -distribution as different conformations show different diffusion rates. Furthermore, at low surface coverage, the average number of lipids that interact with one peptide molecule is expected to be maximized, causing the peptide to be less mobile and hence a slower diffusion time. On the other hand, at high

surface coverage (e.g., at 1 μ M peptide concentration), the surface-bound peptides are more densely packed and thus experience self-crowding. As a result, each peptide molecule interacts, on average, with a smaller number of lipid molecules, making the molecules in the ensemble look alike in terms of their interactions with the membrane. Therefore, the τ_D -distribution becomes narrower and the peptides diffuse, on average, faster. In fact, the major component of the τ_D -distribution obtained at 1 μ M pHLIP (Fig. 4 C) almost coincides with that of the lipids in the membrane (Fig. 5), which further corroborates the idea that at high surface coverage each peptide is interacting with fewer lipids. The above assessments are also consistent with a previous study by Engelman and co-workers, albeit in a qualitative manner, which showed that at pH 8 the interactions between pHLIP and POPC membranes depend on the peptide/lipid ratio (47). By analyzing the free energy change associated with binding of pHLIP to POPC bilayers at different peptide/lipid

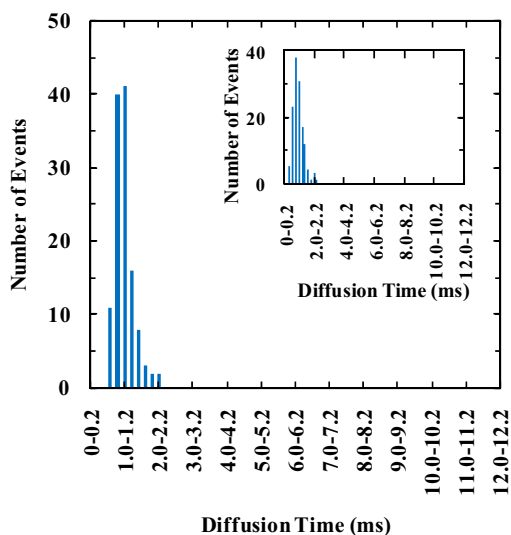


FIGURE 5 Diffusion time (τ_D) distribution of Texas Red-DHPE (0.002 mol %) in GUV membranes at pH 8. (Inset) Diffusion time (τ_D) distribution of Texas Red-DHPE (0.002 mol %) in GUV membranes at pH 4.

ratios, they concluded that there are two types of pHLIP-membrane interactions. Specifically, their results suggest that when the peptide/lipid ratio is low enough so that the entire peptide chain can interact with the membrane, type II interaction dominates and one peptide interacts (on average) with 124 lipid molecules. On the other hand, at high peptide/lipid ratios wherein the total accessible membrane surface area is not large enough to prevent peptide self-crowding, the membrane-bound peptides adopt a bent conformation wherein only part of the peptide chain is interacting with the membrane. In this partial, or type I interac-

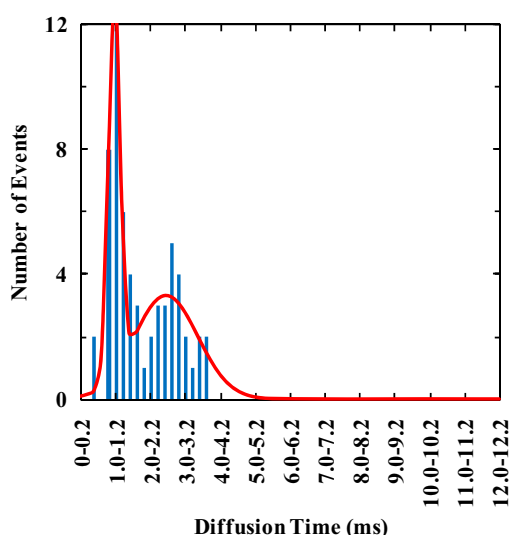


FIGURE 6 Diffusion time (τ_D) distribution of Texas Red-DHPE (0.002 mol %) in GUV membranes with the presence of 1 μ M pHLIP (total concentration) at pH 8.

tion, one peptide interacts with 57 lipids, on average (47). In addition, our results are in agreement with those of Liu et al. (64), who have shown that the diffusivity of a series of homologous amphiphilic molecules on model membranes depends on their size and position. In particular, their results show that the diffusion constant of those amphiphiles that reside near the membrane surface decreases with increasing the molecular surface area. In other words, the diffusivity of an adsorbate molecule depends on the number of lipids it is interacting with or its interfacial area.

Because the present pHLIP peptide carries a net charge of -6 at pH 8, its diffusion behavior is expected to depend on the electrostatics of the membrane. Indeed, addition of negatively charged lipids (i.e., POPG) to the POPC membrane affects the τ_D -distribution of pHLIP. As shown (Fig. S12), the τ_D -distribution exhibits a weaker dependence on (bulk) peptide concentration, as compared to that obtained with zwitterionic POPC membranes. Because at pH 8 pHLIP is expected to have a weaker affinity toward negatively charged membranes and hence a lower membrane surface coverage for a given peptide concentration, this result thus corroborates the aforementioned notion that the peptide density on the membrane surface is one of the key determinants of its diffusion heterogeneity.

Peptide adsorption is expected to also affect the mobility of the membrane lipids, especially those that are directly interacting with the adsorbate molecules. Indeed, the τ_D -distribution of the lipids, which is determined by measuring the diffusion time of a very small number of fluorescently-labeled lipids that are added into the membrane of GUVs, depends on whether pHLIP is absent (Fig. 5) or present (Fig. 6). As shown (Fig. 6), in the presence of 1 μ M pHLIP the τ_D -distribution of the lipids consists of two distinct components, centered at ~ 1.0 and 2.6 ms, respectively. It is apparent that the fast component is similar to that observed when pHLIP is absent and that the entire distribution is similar to the τ_D -distribution of the peptide (i.e., Fig. 4 C) obtained under the same conditions. Thus, these results suggest that the surface-bound pHLIP molecules are moving together, as a loosely packed cluster, with the lipids with which they interact. Similar to what is observed here, a previous study by Zhang and Granick (52) has shown that when the number of lipids that interact with one surface-bound polymer molecule is >80 , the diffusion of the lipids is slaved to the diffusion of the adsorbed substrates and is slow, whereas when the number of lipids that interact with one polymer molecule is <80 , the lipids diffuse faster with a rate similar to that of unperturbed lipids.

Diffusion of transmembrane-bound pHLIP molecules

The diffusion times of the TM-bound pHLIP, obtained at pH 4, show a single distribution which is insensitive to the peptide concentration (Fig. 4, D–F). This result suggests

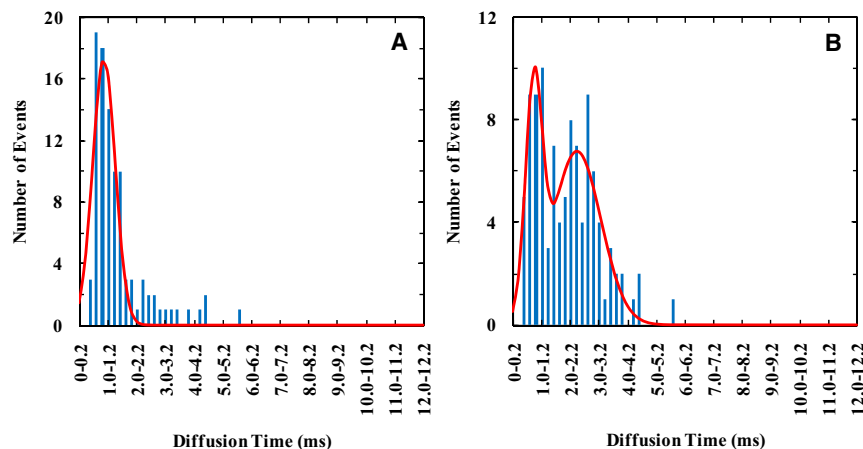


FIGURE 7 Diffusion time (τ_D) distributions of Texas Red-DHPE (0.002 mol %) in GUV membranes with the presence of (A) 1 nM and (B) 1 μ M pHLIP (total concentration) at pH 4.

that the TM-bound pHLIP samples one conformational ensemble, a picture that is consistent with the study of Engelman and co-workers (45–47). However, the τ_D -distribution is still considerably broader than that (i.e., Fig. 5) obtained with unperturbed lipids, indicative of heterogeneity in pHLIP diffusion. Because, under the current experimental conditions, pHLIP does not form aggregates or oligomers (45), this broad τ_D -distribution thus manifests the heterogeneity in the solvation of the TM-bound pHLIP by lipid molecules. To provide further insights into this point, we measured the mobility of the lipids in the presence of pHLIP at pH 4. As shown (Fig. 7), the τ_D -distributions of the lipids obtained at different peptide/lipid ratios show that the mobility of certain lipid molecules is affected by the presence of pHLIP. At 1 μ M peptide concentration, it is apparent that a slow diffusion component emerges as a result of peptide-membrane interactions. Based on the Saffman and Delbruck model (64–66), a diffusing object that shows a diffusion time comparable to the slow diffusion component would have a radius in the range of 1.0–3.0 nm, which was estimated to be equivalent to a diffusing species consisting of one pHLIP molecule and 6–26 lipids (assuming that the radius of the α -helix and that of the lipid headgroup are 0.6 and 0.5 nm, respectively, and that the lipids are tightly packed). Remarkably, this simple estimate is in excellent agreement with the result of Engelman and co-workers (47) that a single TM-bound pHLIP is solvated by 9–16 lipid molecules, distributed in two solvation layers surrounding the α -helix, thus further demonstrating the sensitivity, as well as the uniqueness, of the FCS method in studying peptide-membrane interactions. In addition, we believe that this technique is potentially applicable to probe the transiently populated local lipid clusters in membranes (67).

CONCLUSIONS

In summary, we have measured the diffusion times (or rates) of a membrane-bound pHLIP peptide through a well-defined confocal volume under different conditions. Our results

show that the lateral mobility of this peptide in membranes depends on its conformation as well as its location. When the peptide is adsorbed to the membrane surface where it is unstructured and thus can sample a large number of conformations, individual molecules can show very different diffusion times although the shape and position of the diffusion time distribution depends on the peptide/lipid ratio or surface coverage of the peptide. At sufficiently low peptide/lipid ratios where individual peptide molecules do not experience self-crowding, the diffusion time distribution is composed of one component. Interestingly, increasing the peptide/lipid ratio causes an increase in the average diffusion rate of the surface-bound peptides but a decrease in the width of the distribution. Moreover, at high peptide/lipid ratios, the diffusion time distribution is composed of two distinct components, indicating that under such conditions two distinguishable (by the current method) conformational ensembles are populated. In particular, at sufficiently high peptide/lipid ratios, the diffusion time of the fast diffusion component of the peptide approaches that of the lipid in the membrane. On the other hand, under conditions where the peptide adopts a TM-oriented α -helical conformation, the diffusion time distribution is independent of the peptide/lipid ratio, indicating that the binding of the peptide perturbs fewer lipid molecules. Taken together, these results show that FCS is a useful technique for revealing the conformational heterogeneity of membrane-bound peptides or proteins and that the characteristic FCS diffusion time is a good indicator of how many lipid molecules are interacting with the diffusing species.

SUPPORTING MATERIAL

Fifteen figures are available at [http://www.biophysj.org/biophysj/supplemental/S0006-3495\(10\)00418-2](http://www.biophysj.org/biophysj/supplemental/S0006-3495(10)00418-2).

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